

Numerical Evaluation of the Polarizability Tensors of Stem Cells with Realistic 3D Shapes

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NIST

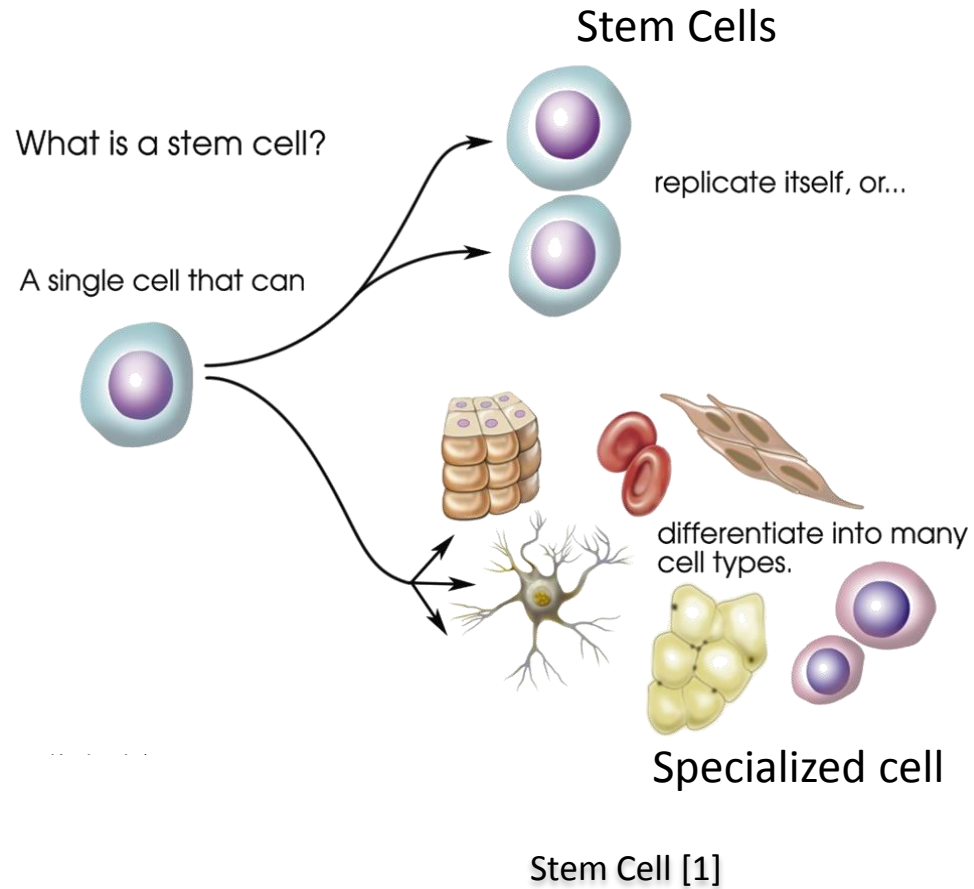
National Institute of
Standards and Technology
U.S. Department of Commerce

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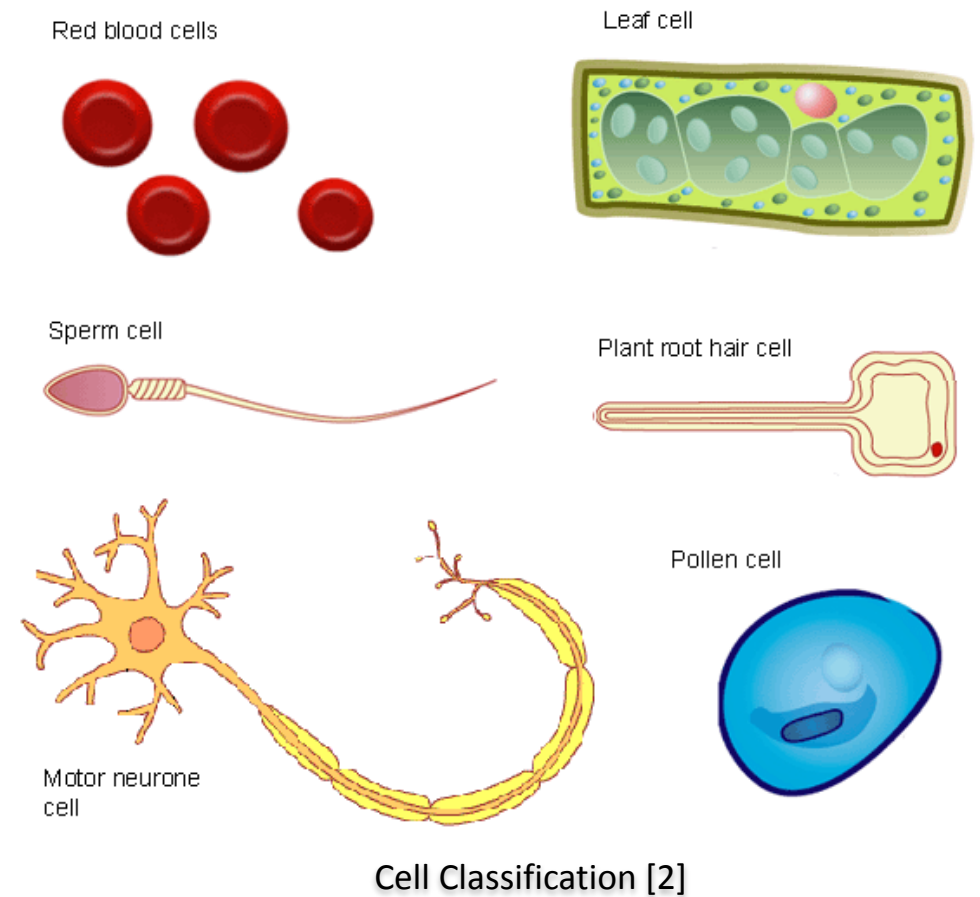
(1-17)

Introduction

Stem Cells differentiate into cells with different shape and functionality



Variation in cell shape or morphology is analyzed in cell classification and cancer diagnosis study

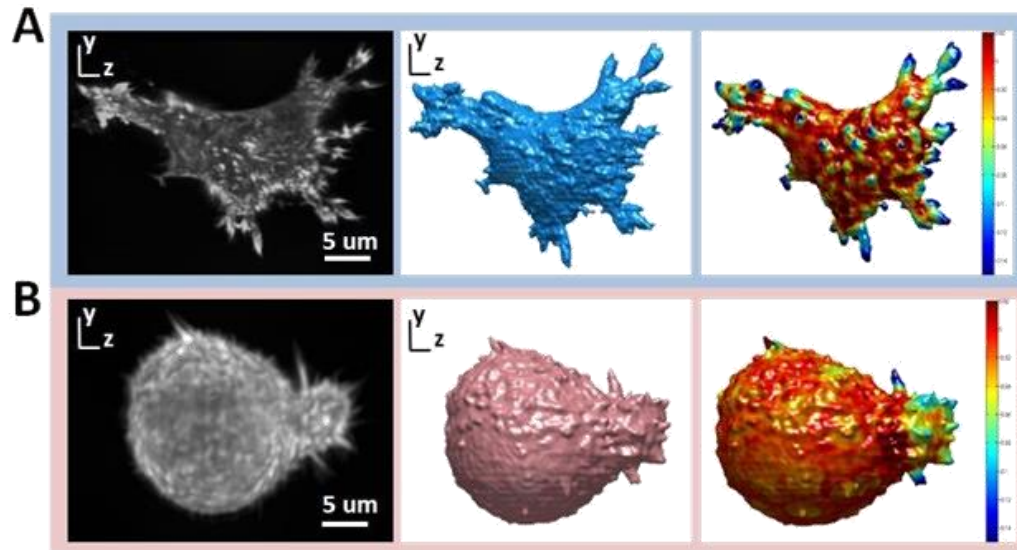


[1] Catherine Twomey; Understanding Stem cells: An Overview of the Science and Issues from the National Academies, <http://www.nationalacademies.org/stemcells>

[2] Haleo.co.uk. (2017). <http://haleo.co.uk/the-body/cells/>

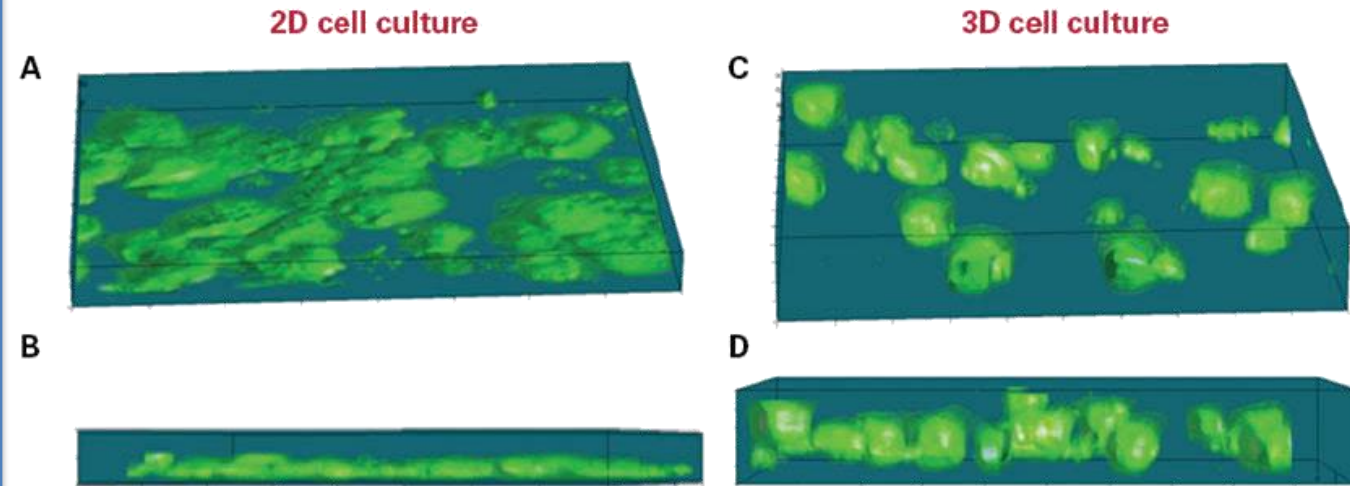
Imaging of 3D Cell Shapes

- Accurately capture the geometric parameters such as: 3D shape, volume and surface area
- Overcomes the dependency on orientation and focal plane of the image
- Helps determine the exact location of nuclei



3D Morphology of two biological cells [1]

- Growth of cells in a 2D environment during imaging can lead the cells to acquire an artificial flattened shape that does not reflect the true 3D shape of the cell in its natural environment



Cell Growth in 3D & 2D substrate[2]

[1] Utsouthwestern.edu. (2017). Who We Are: Danuser Lab - UT Southwestern, Dallas, Texas. <http://www.utsouthwestern.edu/labs/danuser/who-we-are/>

[2] Reinnervate.com. (2017). What is Alvetex? • ReproCELL Europe. <http://reinnervate.com/alvetex/about-alvetex/what-is-alvetex/>

NIST 3D Stem Cells Database

- NIST studied different scaffold systems to provide a 3D microenvironment that enables cells to behave more physiologically
- 3D confocal microscopy and 3D image analyses were used to reconstruct the 3D shapes of the cells
- 10 different environments (Scaffolds or planar substrates) with at least 100 cells per environment



3D Measurement of Stem Cell-Scaffold Interactions

Based on Cell Shapes

- Stem cell-scaffold on-line interactions
- Download web page for raw and processed z-stacks

<https://isg.nist.gov/deepzoomweb/data/stemcellmaterialinteractions>

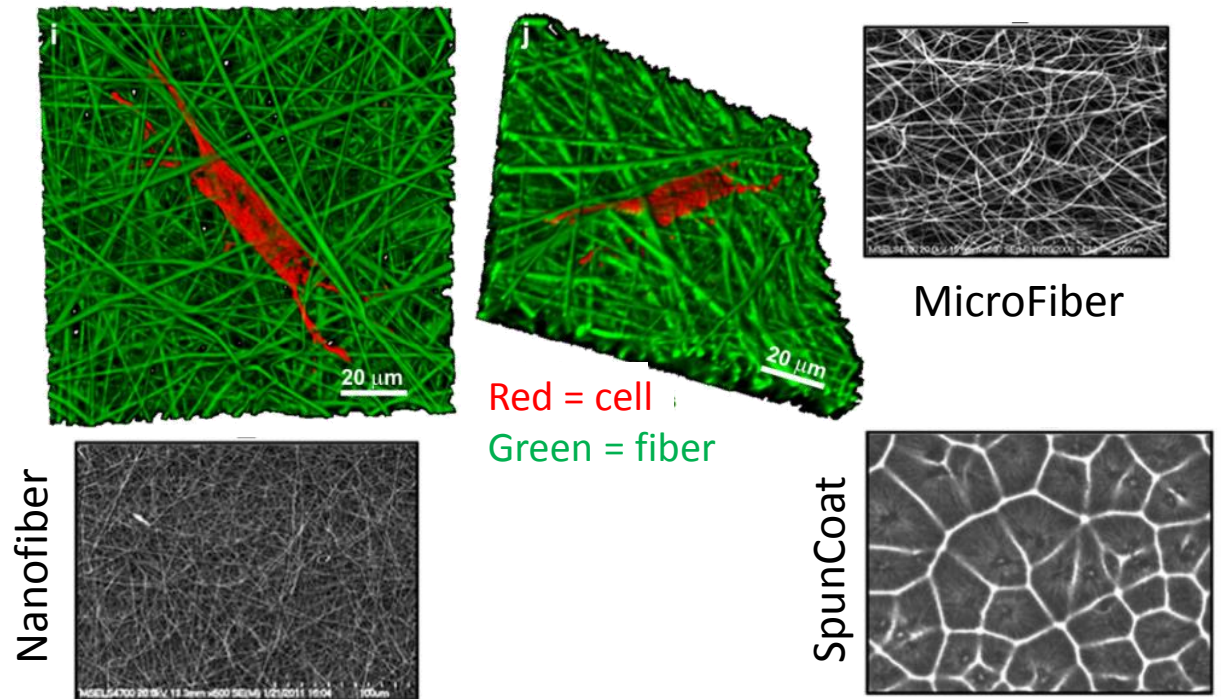


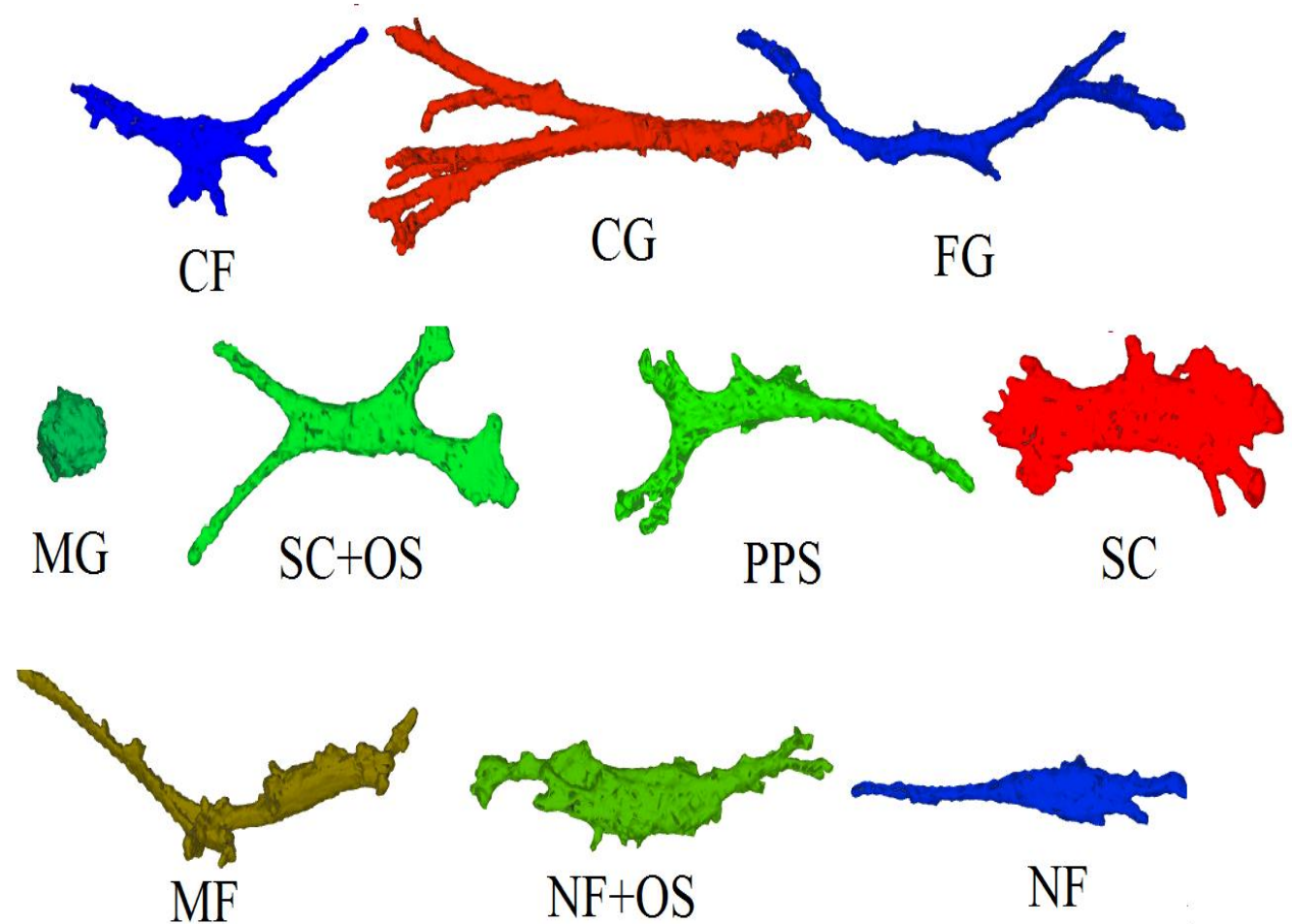
Fig: Cell Growth in Nanofiber scaffold and 3 different scaffold [1,2]

[1] T. M. Farooque, C. H. Camp, C. K. Tison, G. Kumar, S. H. Parekh, and C. G. Simon, "Measuring stem cell dimensionality in tissue scaffolds," *Biomaterials*, vol. 35, no. 9, pp. 2558–2567, Mar. 2014.

[2] Kumar, Girish, et al. "The determination of stem cell fate by 3D scaffold structures through the control of cell shape." *Biomaterials* 32.35 (2011): 9188-9196.

NIST 3D Stem Cells Database

- 3 families used a polymer based microenvironment: SpunCoat (SC), Nanofibers (NF), Microfibers (MF)
- 3 families used hydrogels from different sources: Matri-Gel (MG), Fibrin Gel (FG), and Collagen Gel (CG)
- Two families prepared from collagen: Collagen Gel (CG), Collagen Fibrils (CF)
- Osteogenic supplements (OS) were added to two existing cultures (NF+OS, SC+OS) to assess effect of chemical composition
- Cell shapes are strongly influenced by scaffold properties, scaffolds could drive cells into complex 1D, 2D or 3D shapes



Goal of this work is to study the electric properties of these cells with realistic 3D shapes

Static Electric Polarizability

- The static polarizability tensor describes the capability of a certain body to experience charge separation, forming a dipole moment, in response to an incident electric field

$$p = \alpha E$$

$$\begin{bmatrix} P_x \\ P_y \\ P_z \end{bmatrix} = \begin{bmatrix} \alpha_{xx} & \alpha_{xy} & \alpha_{xz} \\ \alpha_{yx} & \alpha_{yy} & \alpha_{yz} \\ \alpha_{zx} & \alpha_{zy} & \alpha_{zz} \end{bmatrix} \begin{bmatrix} E_x \\ E_y \\ E_z \end{bmatrix}$$

- Non-uniform cell geometry requires the **Numerical** solution of the following Laplace's Equation to calculate the polarizability tensors

$$\nabla^2 V(r) = 0$$

$$\alpha = \begin{bmatrix} \alpha_{xx} & \alpha_{xy} & \alpha_{xz} \\ \alpha_{yx} & \alpha_{yy} & \alpha_{yz} \\ \alpha_{zx} & \alpha_{zy} & \alpha_{zz} \end{bmatrix} \xrightarrow{\text{Diagonalization}} \hat{\alpha} = \begin{bmatrix} \hat{\alpha}_1 & 0 & 0 \\ 0 & \hat{\alpha}_2 & 0 \\ 0 & 0 & \hat{\alpha}_3 \end{bmatrix}$$

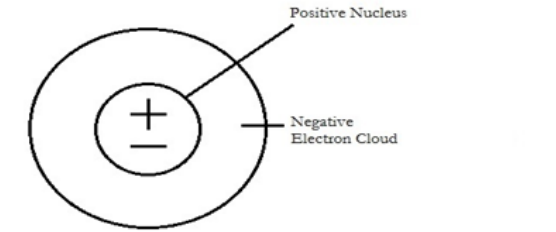


Fig 3.12A: Atom before being placed in Electric Field

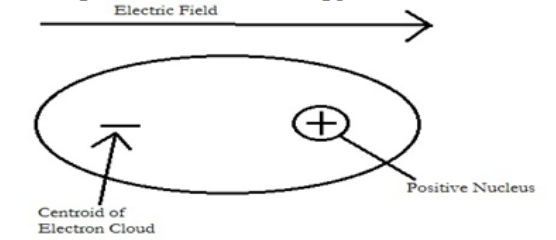
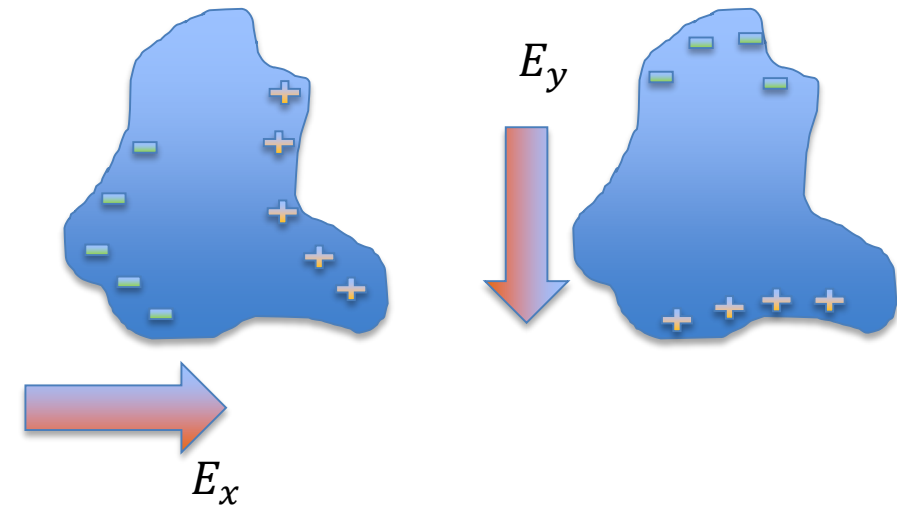
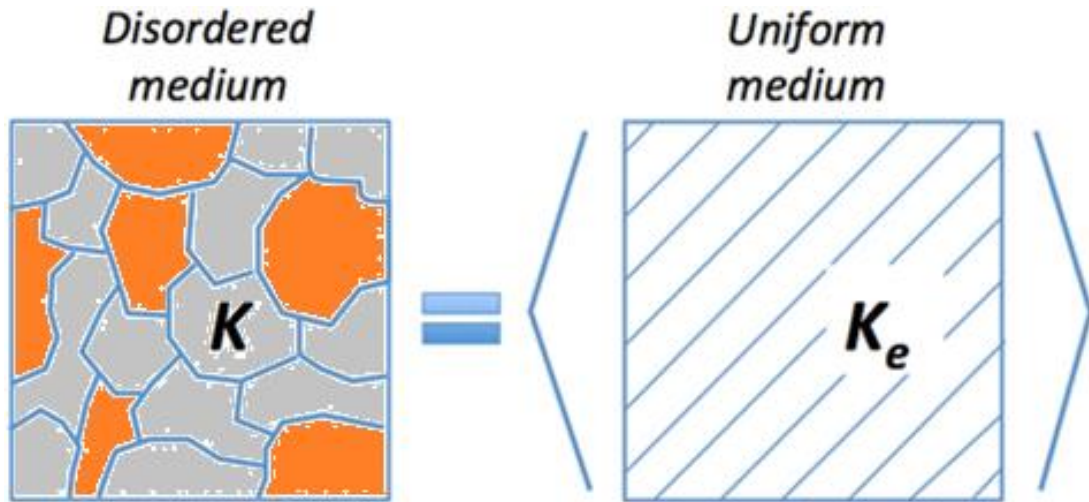


Fig 3.12B: Atom placed in Electric Field

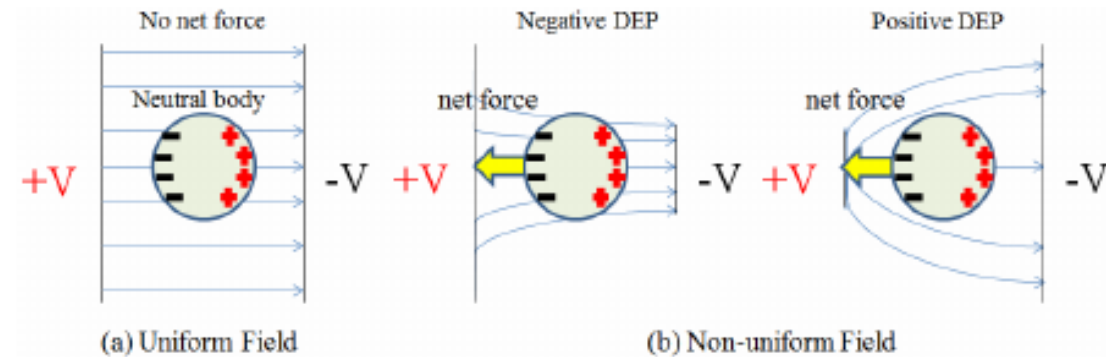
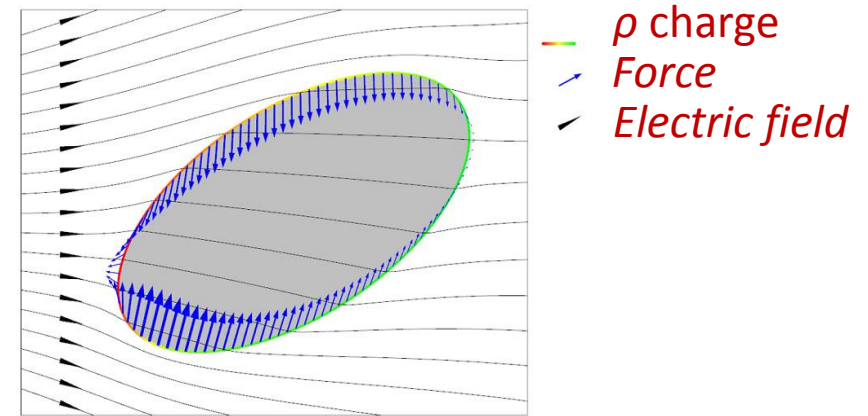


Application of Polarizability Tensor

- The effective electrical properties of composite materials i.e. tissue



- Dielectrophoresis: Motion of a cell due to an incident inhomogeneous electric field



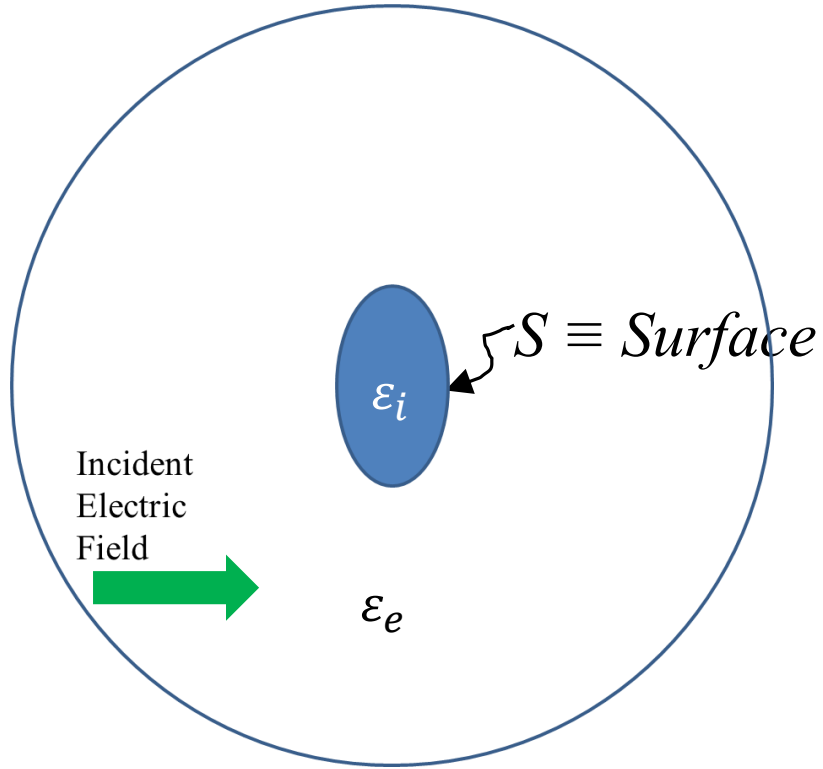
$$\text{Dielectrophoretic Force, } \vec{F}_{DEP} = \frac{1}{2} \alpha V (\nabla E^2)$$

[1] Ghanbarian, Behzad, and Hugh Daigle. "Permeability in two-component porous media: Effective-medium approximation compared with lattice-Boltzmann simulations." *Vadose Zone Journal* 15.2 (2016).

[2] Kim, Dong, et al. "Effect of array and shape of insulating posts on proteins focusing by direct current dielectrophoresis." *Journal of Mechanical Science and Technology* 28.7 (2014): 2629.

Calculation of the Polarizability Tensors

Electric Polarizability Tensor (α_E)



$$p = \int_V P dV = (\epsilon_i - \epsilon_e) \iiint E_i dV$$

The screenshot shows the COMSOL Multiphysics interface. The 'Model Builder' tree on the left shows the 'Form Union' and 'Form Composite' objects highlighted with red boxes. The 'Results' window on the right shows 'Derived Values' with 'Volume Integration 1' and 'Volume Integration 3' selected. The 'Expression' field for 'Volume Integration 1' is highlighted with a red box and contains the formula $(\text{mat2}-1)*\text{es.Ex}/15127$. The 'Description' field for 'Volume Integration 1' contains the formula $(\text{mat2}-1)*\text{es.Ex}/V$. A red arrow points from the equation in the diagram to the expression in the software.

Electrostatic Solvers

➤ To validate our results for these complex cell shapes, the following independent solvers were employed:

1. COMSOL: Commercial Finite Element Package

(Tetrahedral discretization)

2. SCUFF-EM: Open Source Method of Moments

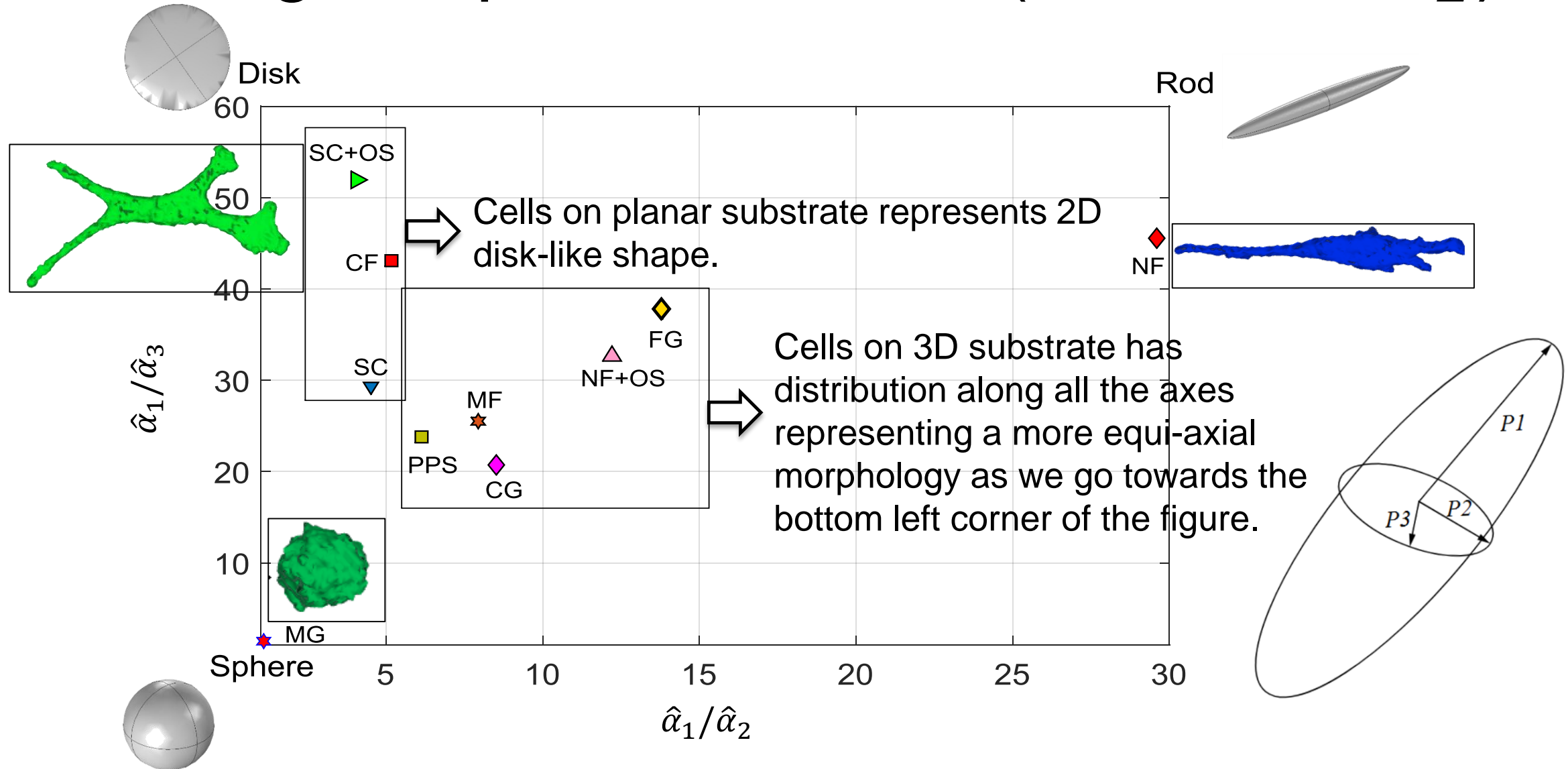
(Surface triangular mesh)

| Cell Family | α_e | Scuff-EM | COMSOL | Percentage Uncertainty |
|------------------|------------------|----------|---------|------------------------|
| PPS | $\hat{\alpha}_1$ | 86.4257 | 84.4609 | 2.27% |
| | $\hat{\alpha}_2$ | 14.3076 | 13.6767 | 4.41% |
| | $\hat{\alpha}_3$ | 3.3438 | 3.2124 | 3.93% |
| Collagen Fibrils | $\hat{\alpha}_1$ | 85.726 | 80.2635 | 6.37% |
| | $\hat{\alpha}_2$ | 17.0776 | 16.0936 | 5.76% |
| | $\hat{\alpha}_3$ | 1.7764 | 1.7029 | 4.14% |
| Microfibers | $\hat{\alpha}_1$ | 99.2096 | 92.6334 | 6.63% |
| | $\hat{\alpha}_2$ | 12.8925 | 12.2077 | 5.31% |
| | $\hat{\alpha}_3$ | 3.8979 | 3.7389 | 4.08% |

$$\% \text{ Uncertainty} = \frac{|\alpha_{\text{SCUFF_EM}} - \alpha_{\text{COMSOL}}|}{\alpha_{\text{SCUFF_EM}}} * 100$$

Maximum percentage uncertainty for the case of sampling is 6.63%

Encoding Shape Information (Based on α_E)

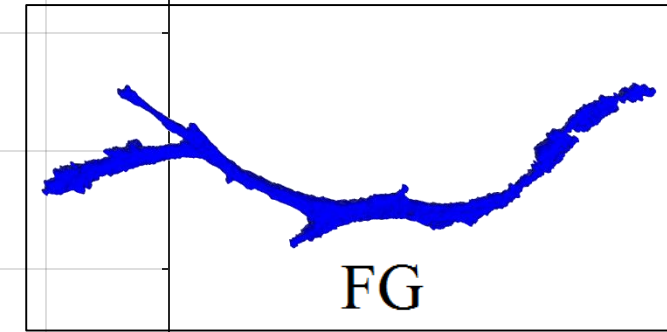
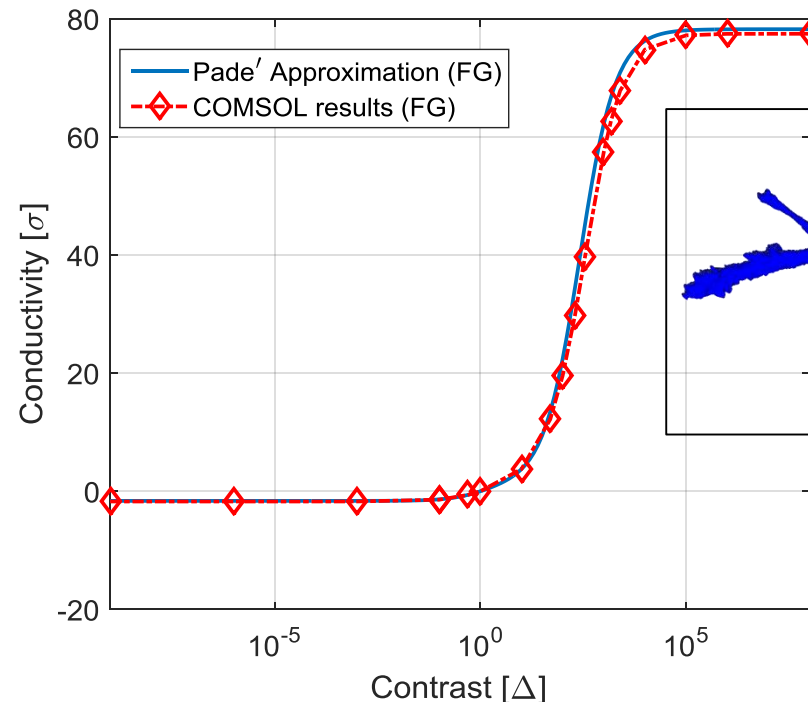
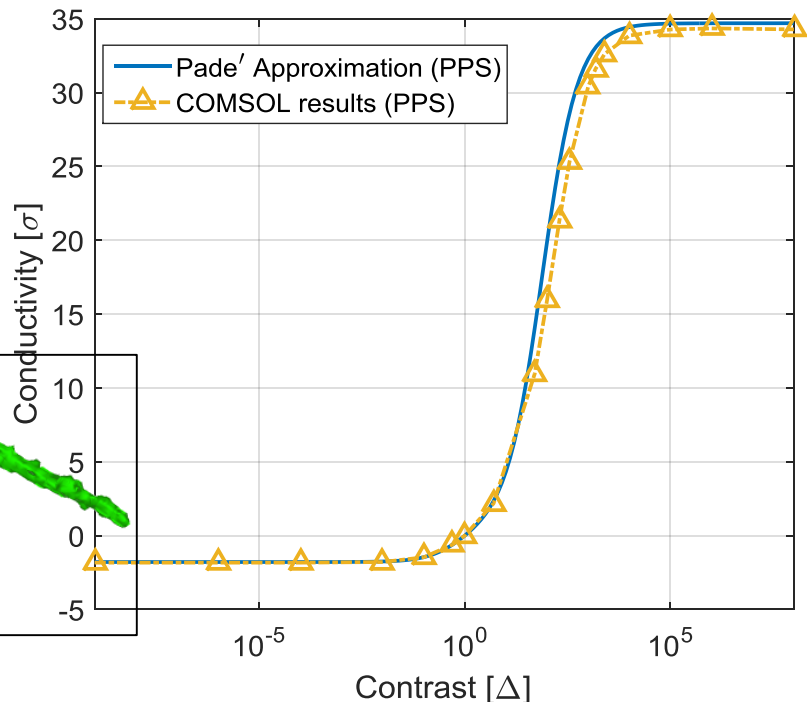
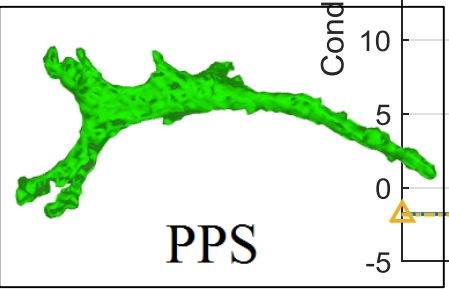
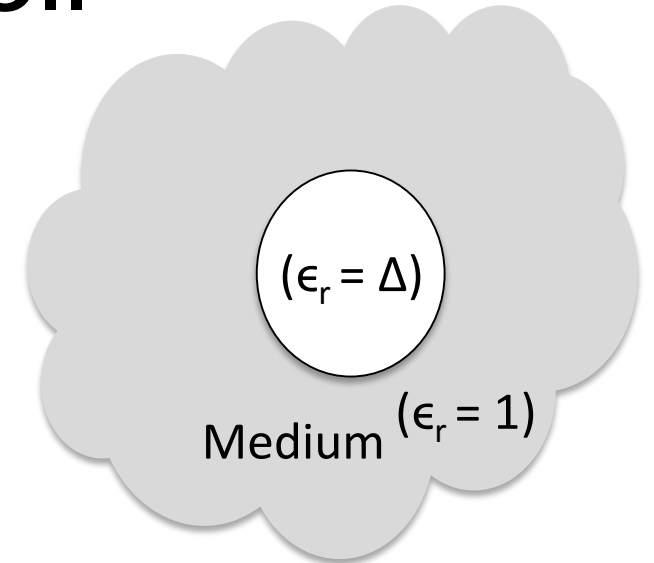


Variable Contrast for cell

Padé approximation $[\sigma(\Delta)] = \frac{[\sigma]_{\infty}(\Delta - 1)^2 + a(\Delta - 1)}{(\Delta - 1)^2 + ([\sigma]_{\infty} + a/d)(\Delta - 1) + a}$

Particle shape dependent constant $a = \frac{[\sigma]_{\infty} - [\sigma]_0 + [\sigma]_{\infty}[\sigma]_0}{1 + (1 - 1/d)[\sigma]_0}$

$$[\sigma]_{\infty} = \frac{1}{3} \text{Tr}(\mathbf{\alpha}_e) \quad [\sigma]_0 = \frac{1}{3} \text{Tr}(\mathbf{\alpha}_m) \quad [\sigma(\Delta)] = \frac{1}{3} \text{Tr}(\mathbf{\alpha})$$



Conclusions

- Stem cells electrical properties, such as polarizability, is affected by the culturing environment and are significantly different from those of a sphere or ellipsoid
- The electrostatic characteristics can be used as a 3D cell shape classifier
- The Padé approximation provides an accurate and a computationally inexpensive way to calculate the polarizability at any contrast

References

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Minimum Enclosing Ellipse (α_E clustering)

The general form of an ellipsoid in center form

$$\mathcal{E} = \{x \in \mathbb{R}^n \mid (x - c)^T A (x - c) = 1\}$$

The volume of the ellipsoid

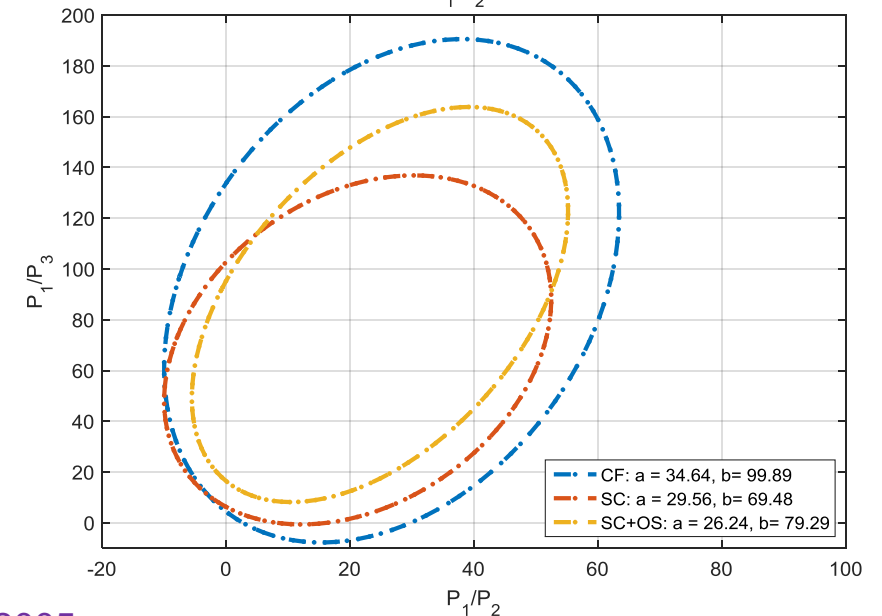
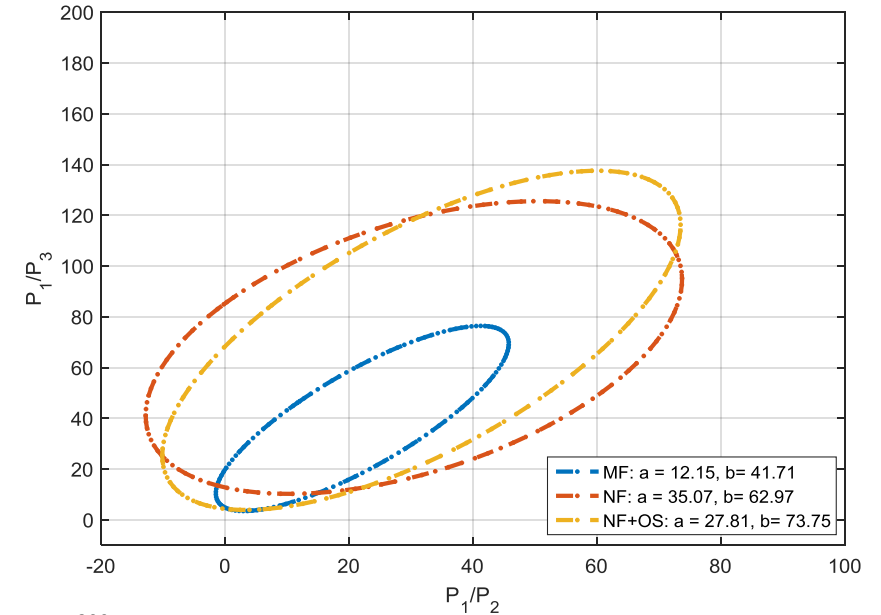
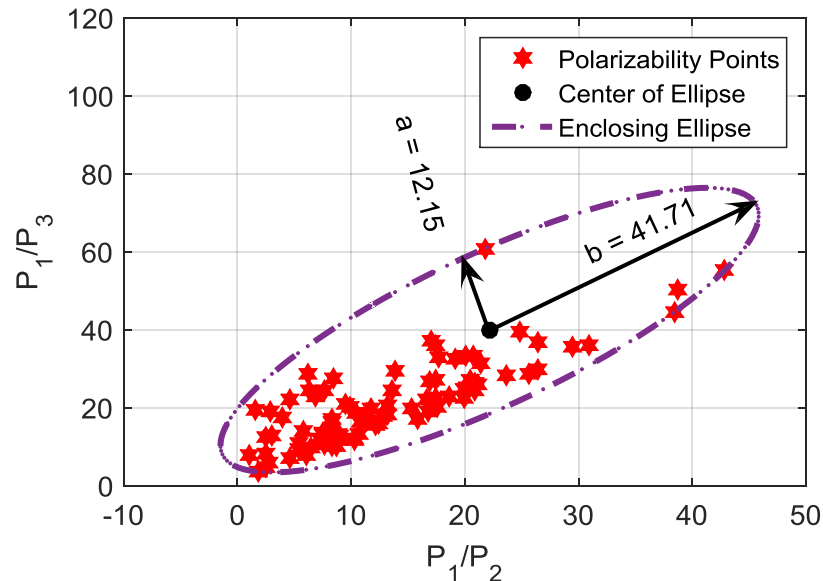
$$Vol(\mathcal{E}) = \frac{v_0}{\sqrt{\det(A)}} = v_0 \det(A^{-1})^{\frac{1}{2}}$$

The optimization problem

$$\text{minimize } \det(E^{-1})$$

Under the constraint

$$(f_i - c)^T A (f_i - c) \leq 1 \quad i = 1, 2 \dots m$$



Polarizability Comparison

Diagonal elements of Electric Polarizability Comparison (α_E)

| Cell Family | α_e | Scuff-EM (Down 4) | COMSOL (Down 4) | Percentage Uncertainty |
|------------------|----------------|-------------------|-----------------|------------------------|
| PPS | P ₁ | 86.4257 | 84.4609 | 2.27% |
| | P ₂ | 14.3076 | 13.6767 | 4.41% |
| | P ₃ | 3.3438 | 3.2124 | 3.93% |
| Collagen Fibrils | P ₁ | 85.726 | 80.2635 | 6.37% |
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| Microfibers | P ₁ | 99.2096 | 92.6334 | 6.63% |
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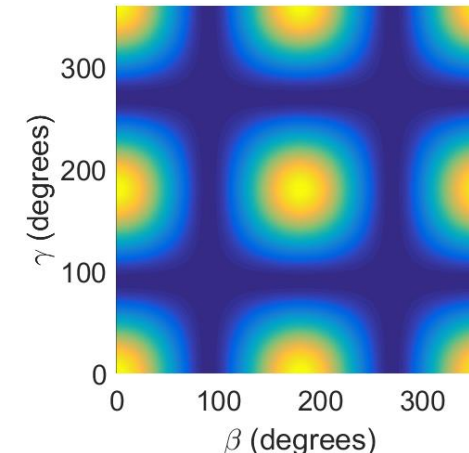
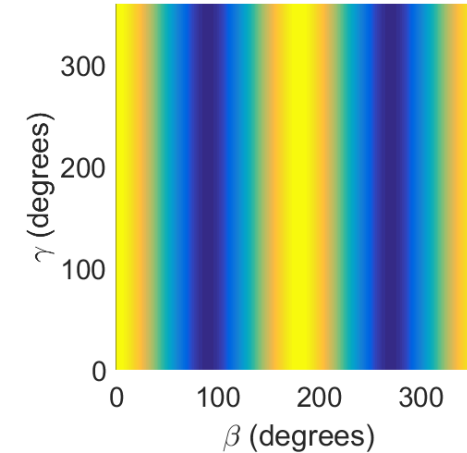
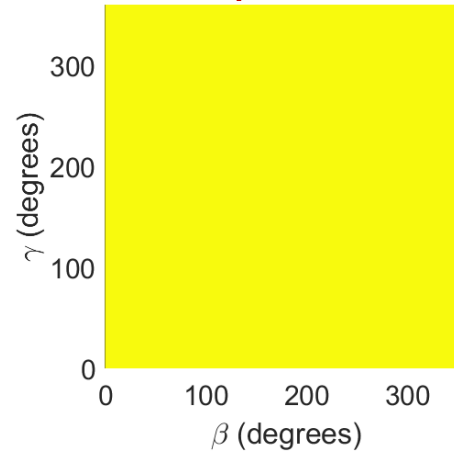
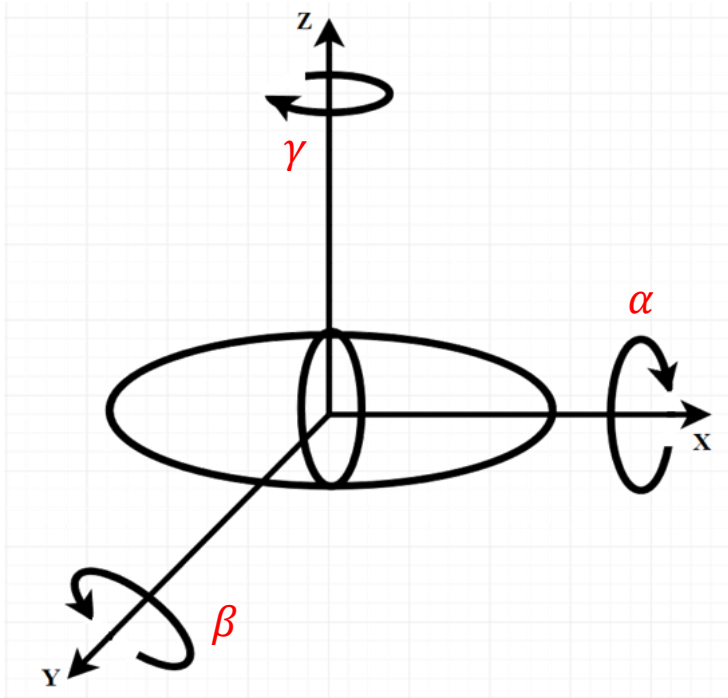
| Cell Family | α_e | Voxel | Scuff-EM (Down 1) | Percentage Uncertainty |
|-------------|----------------|----------|-------------------|------------------------|
| Matrigel | P ₁ | 4.3171 | 4.5036 | 4.14% |
| | P ₂ | 3.9992 | 3.9062 | 2.38% |
| | P ₃ | 3.0494 | 2.9465 | 3.49% |
| NF+OS | P ₁ | 92.648 | 85.06 | 8.92% |
| | P ₂ | 7.4425 | 6.8821 | 8.14% |
| | P ₃ | 2.405 | 2.5791 | 6.75% |
| Microfibers | P ₁ | 136.9432 | 129.8975 | 5.42% |
| | P ₂ | 17.3376 | 16.3612 | 5.97% |
| | P ₃ | 5.0318 | 5.0886 | 1.12% |

$$\% \text{ Uncertainty} = \frac{|\alpha_{\text{SCUFF_EM}} - \alpha_{\text{COMSOL}}|}{\alpha_{\text{SCUFF_EM}}} * 100$$

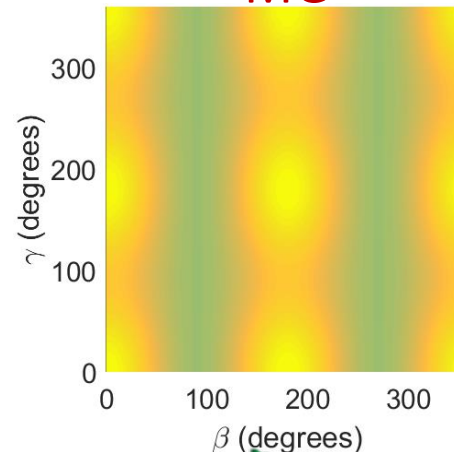
Maximum percentage uncertainty for the case of *Down 4* sampling is **6.63%**
 Maximum percentage uncertainty in case of *Down 1* sampling is **8.92%**.



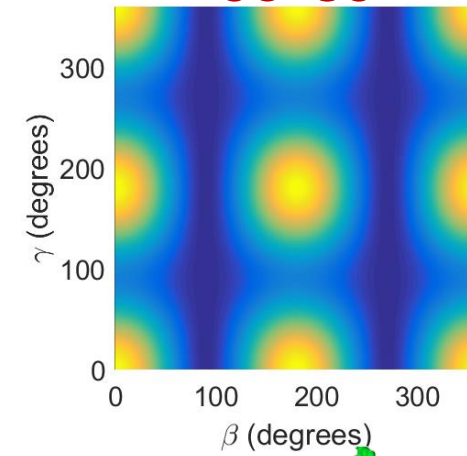
Variation of Polarizability with Cell Rotation



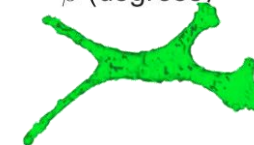
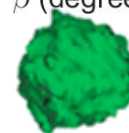
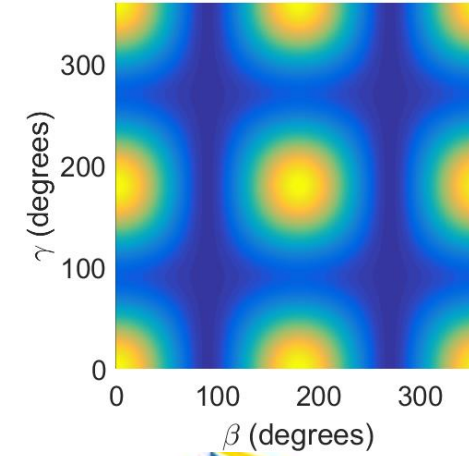
MG



SC+OS



NF



- Plots show variations in α_{Exx} as the cells are rotated around the y-axis and z-axis
- Matrigel (MG) showing very small variation in α_{Exx} showing it is behaving electrically similar too a sphere
- The behavior of SC+OS is closer to an oblate ellipsoid whereas NF is closer to a prolate ellipsoid.

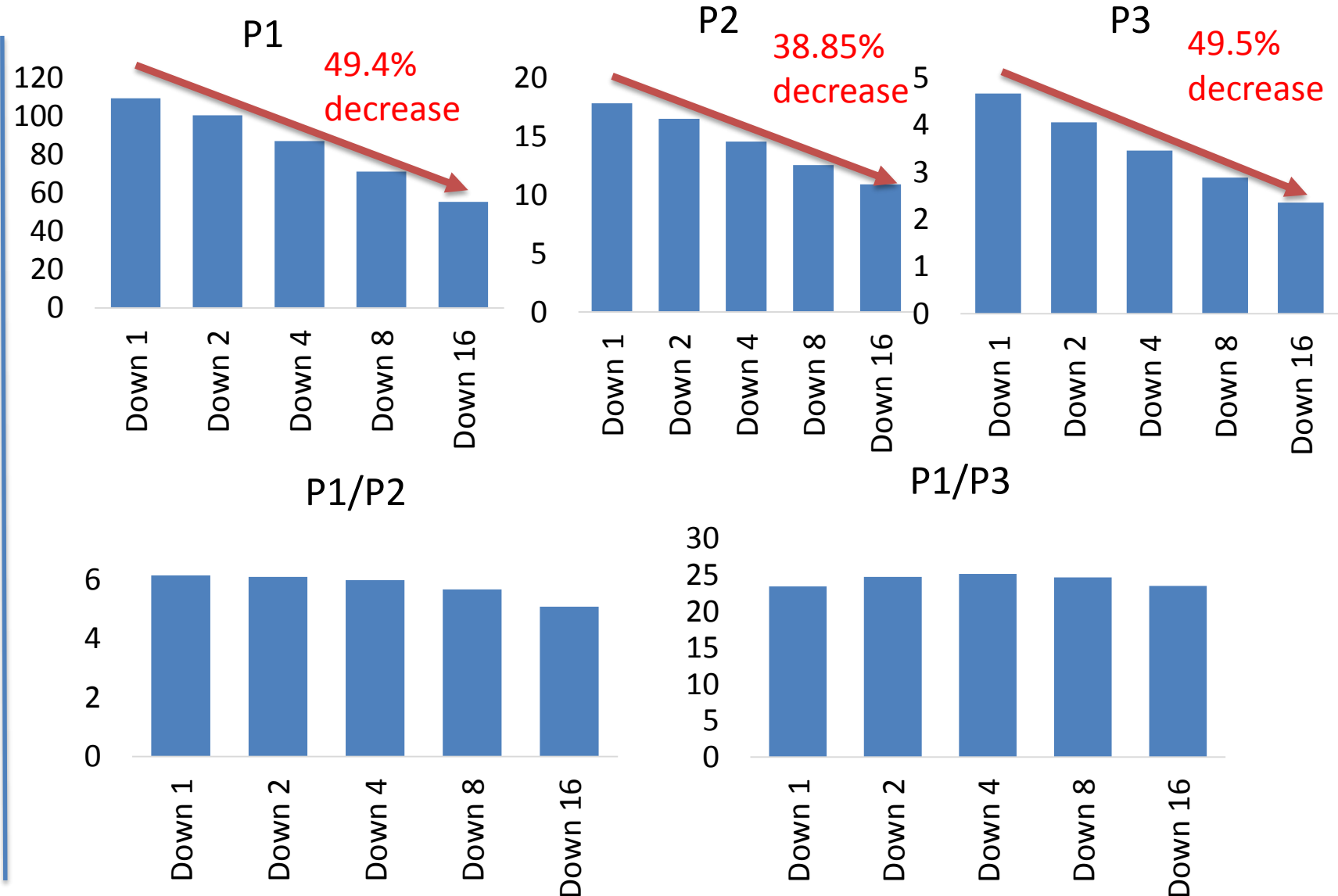
Polarizability VS Meshing Resolution (PPS)

- In general, polarizability matrix α_E has 9 nonzero elements (6 independent elements)
- Polarizability matrix can be diagonalized such that

$$\alpha_E = \begin{bmatrix} \alpha_{Exx} & \alpha_{Exy} & \alpha_{Exz} \\ \alpha_{Eyx} & \alpha_{Eyy} & \alpha_{Eyz} \\ \alpha_{Ezx} & \alpha_{Ezy} & \alpha_{Ezz} \end{bmatrix}$$

$$\text{Diagonalized } \alpha_E = \begin{bmatrix} P_1 & 0 & 0 \\ 0 & P_2 & 0 \\ 0 & 0 & P_3 \end{bmatrix}$$

$$P_1 \geq P_2 \geq P_3$$

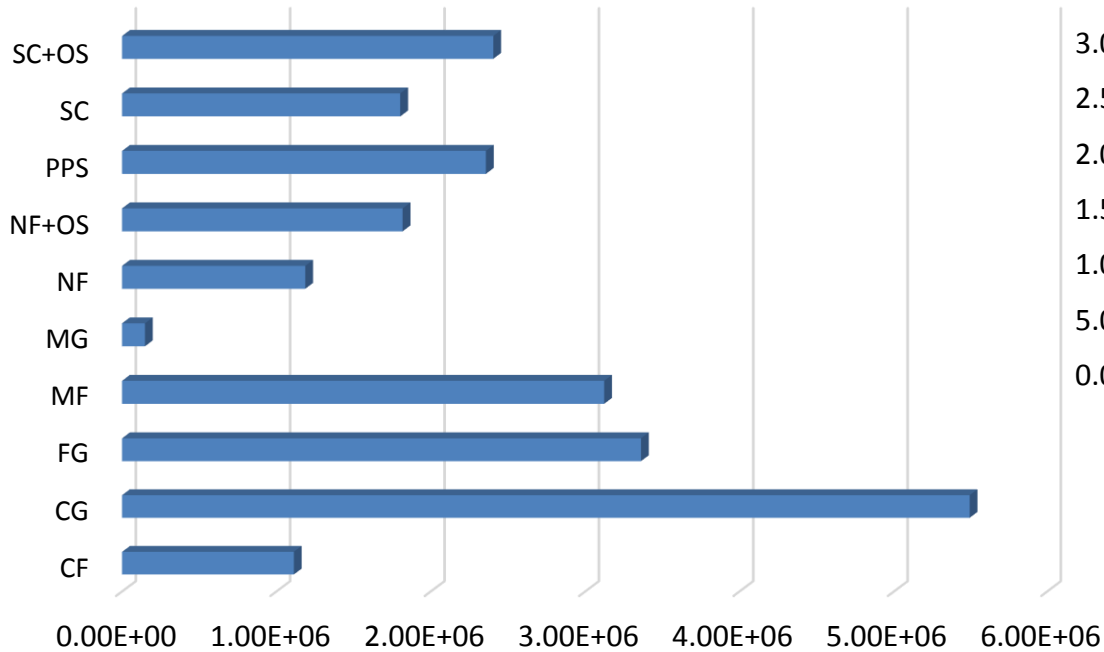


P_1, P_2, P_3 highly sensitive to meshing resolution Ratios P_1/P_3 and P_1/P_2 insensitive to meshing resolution

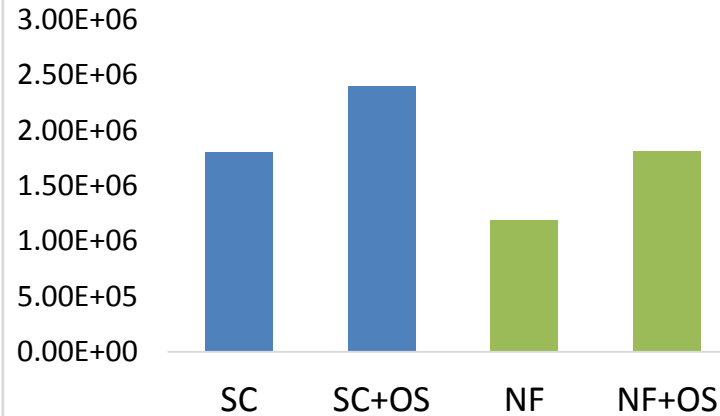
Observation based on the P_{cell}

$$P_{cell} = P_1 + P_2 + P_3$$

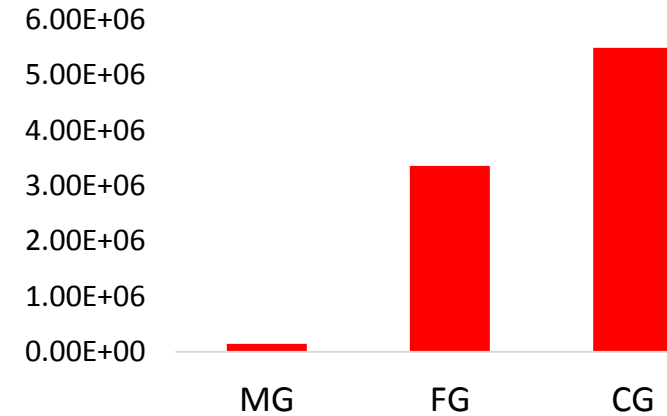
Polarizability (P_{cell})



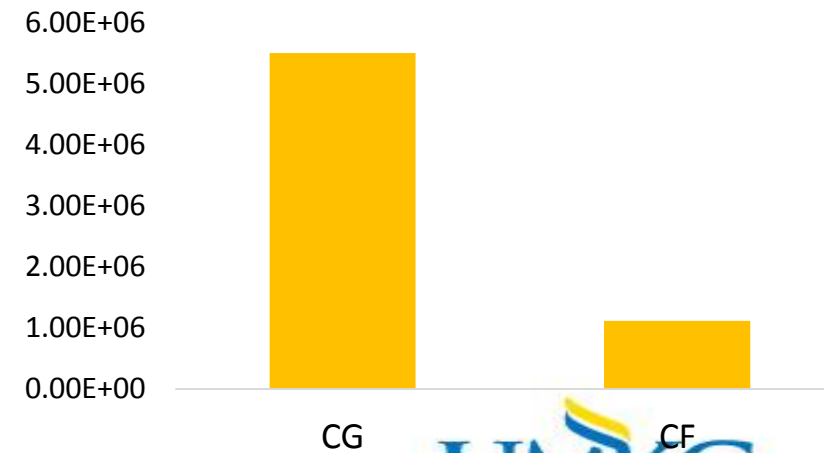
Polarizability Tensor (P_{cell})



Polarizability Tensor (P_{cell})



Polarizability Tensor (P_{cell})



- The addition of OS (osteogenic supplements) caused a significant increase in P_{cell} implying increased exposure to external excitation.
- MG, FG & CG were made from natural hydrogel but still depicting different sensitivity to electrical signals \rightarrow geometry of the microenvironment has an effect on its electrical properties
- Culturing cell on Collagen Fibrils(CF) instead of Collagen Gel (CG) may improve sensitivity to electrical signals (CG).

Polarizability Comparison (Down 4)

Diagonal elements of Electric Polarizability Comparison (α_E)

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| | P ₃ | 3.8979 | 3.7389 | 4.08% |

Magnetic Polarizability Comparison (α_M)

| Cell Family | α_M | Scuff-EM | COMSOL | Percentage Uncertainty |
|------------------|----------------|----------|---------|------------------------|
| PPS | P ₁ | -2.4135 | -2.4364 | 0.95% |
| | P ₂ | -1.7328 | -1.7364 | 0.21% |
| | P ₃ | -1.2249 | -1.2514 | 2.16% |
| Collagen Fibrils | P ₁ | -2.7481 | -2.7811 | 1.20% |
| | P ₂ | -1.4856 | -1.4656 | 1.35% |
| | P ₃ | -1.1768 | -1.1674 | 0.80% |
| Microfibers | P ₁ | -1.9967 | 1.9916 | 0.26% |
| | P ₂ | -1.7402 | -1.7626 | 1.29% |
| | P ₃ | -1.3312 | -1.377 | 3.44% |

$$\% \text{ Uncertainty} = \frac{|\alpha_{\text{SCUFF_EM}} - \alpha_{\text{COMSOL}}|}{\alpha_{\text{SCUFF_EM}}} * 100$$

Maximum percentage uncertainty for the case of α_E is **6.37%**
 Maximum percentage uncertainty in case of α_M is **3.44%**.

Polarizability Comparison (Down 1)

Diagonal elements of Electric Polarizability Comparison (α_E)

| Cell Family | α_e | Voxel | Scuff-EM | Percentage Uncertainty |
|-------------|----------------|----------|----------|------------------------|
| Matrigel | P ₁ | 4.3171 | 4.5036 | 4.14% |
| | P ₂ | 3.9992 | 3.9062 | 2.38% |
| | P ₃ | 3.0494 | 2.9465 | 3.49% |
| NF+OS | P ₁ | 92.648 | 85.06 | 8.92% |
| | P ₂ | 7.4425 | 6.8821 | 8.14% |
| | P ₃ | 2.405 | 2.5791 | 6.75% |
| Microfibers | P ₁ | 136.9432 | 129.8975 | 5.42% |
| | P ₂ | 17.3376 | 16.3612 | 5.97% |
| | P ₃ | 5.0318 | 5.0886 | 1.12% |

Magnetic Polarizability Comparison (α_M)

| Cell Family | α_M | Voxel | Scuff-EM | Percentage Uncertainty |
|-------------|----------------|---------|----------|------------------------|
| Matrigel | P ₁ | -1.8174 | -1.7597 | 3.28% |
| | P ₂ | -1.5781 | -1.5293 | 3.19% |
| | P ₃ | -1.4794 | -1.4289 | 3.53% |
| NF+OS | P ₁ | -3.246 | -2.981 | 8.89% |
| | P ₂ | -1.6968 | -1.6521 | 2.71% |
| | P ₃ | -1.2262 | -1.2308 | 0.37% |
| Microfibers | P ₁ | -2.2754 | -2.2205 | 2.47% |
| | P ₂ | -1.7542 | -1.6648 | 5.37% |
| | P ₃ | -1.5092 | -1.439 | 4.88% |

$$\% \text{ Uncertainty} = \frac{|\alpha_{\text{SCUFF_EM}} - \alpha_{\text{Voxel}}|}{\alpha_{\text{SCUFF_EM}}} * 100$$

Maximum percentage uncertainty for the case of α_E is **8.92%**
 Maximum percentage uncertainty in case of α_M is **8.89%**.

Magnetic Polarizability

